



#### SIMULATION D'IRM ANGIOGRAPHIQUE PAR EXTENSION DU LOGICIEL JEMRIS



#### **Alexandre FORTIN**

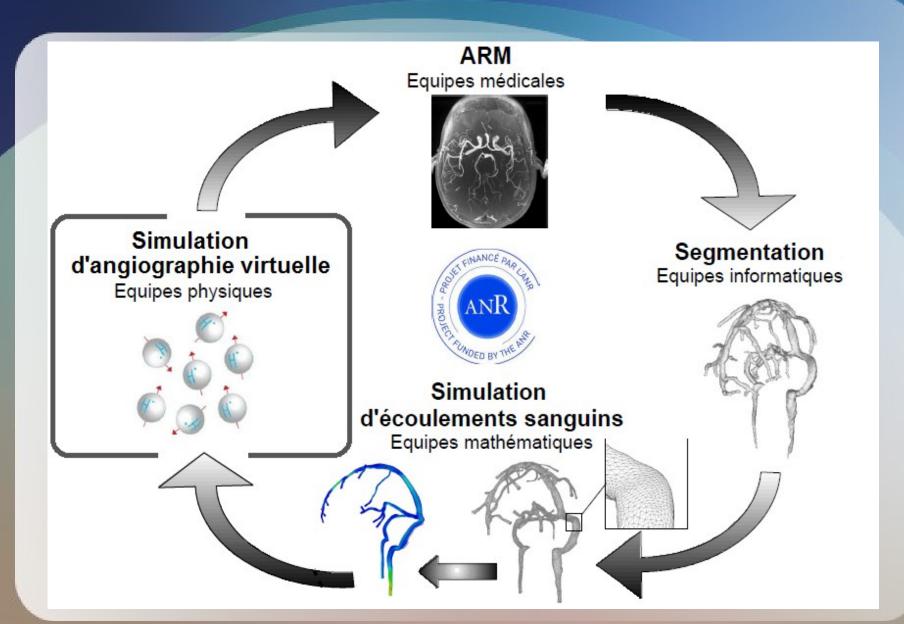
Supervised by Emmanuel DURAND

and Stéphanie SALMON

Laboratoire de Mathématiques de Reims

Model : clipart-fr.com

### **VIVABRAIN PROJECT**





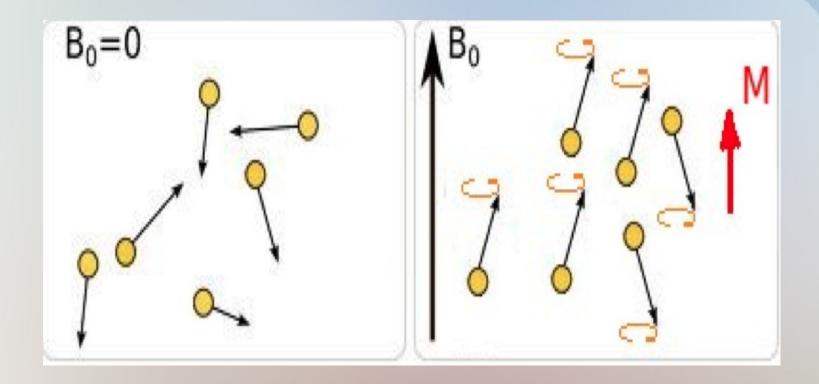
**Schematically**:

MRI machine = a magnet + radio antennas



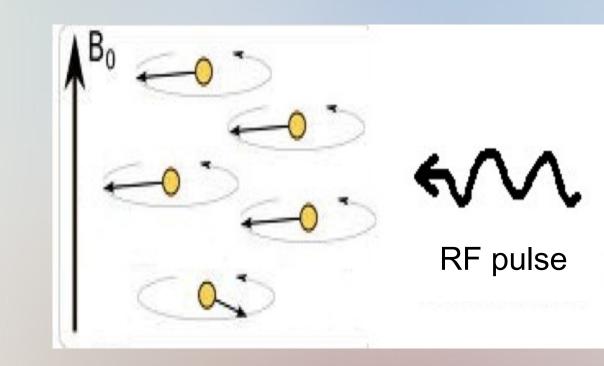
### PHYSICAL BASIS OF MRI

# **# A magnet :** to generate macroscopic magnetization in tissues



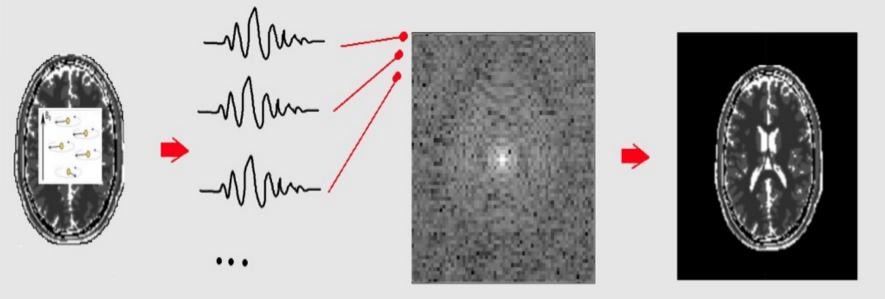
### PHYSICAL BASIS OF MRI

### # Radio antennas : to excite protons with RF pulses and to collect MR signal



### PHYSICAL BASIS OF MRI

## **Building image from MR signal**



Sample

MR signal

Fourier plane

Image (after 2D Fourier transform)

#### **Motivations :**

- Education, understanding MRI physics
- **Optimization** of MRI sequences
- Validation of physic models (CFD models for us)

Conducting experiments difficult in reality

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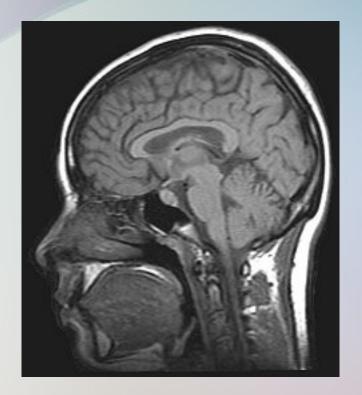
- *Education*, understanding MRI physics
- **Optimization** of MRI sequences
- **Validation** of physic models (CFD models for us)
- **Conducting experiments** impossible in vivo

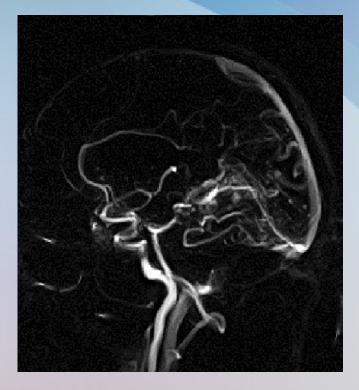


#### Some advanced MRI simulators (mostly open-source)

JEMRIS, ODIN, SIMRI, POSSUM...

### POSITION OF THE PROBLEM





What simulators can do (static

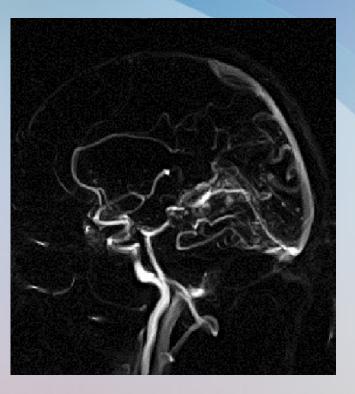
tissues)

What we expect (angiographic images)

### POSITION OF THE PROBLEM

#### Necessity to simulate complex

#### blood movements



What we expect (angiographic images)

### POSITION OF THE PROBLEM

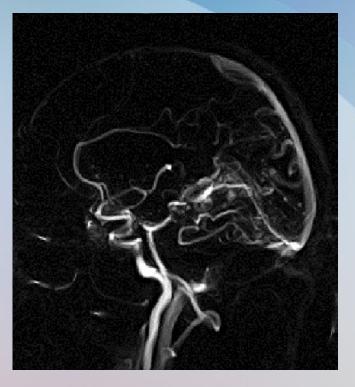
#### Necessity to simulate complex

blood movements



Not implemented

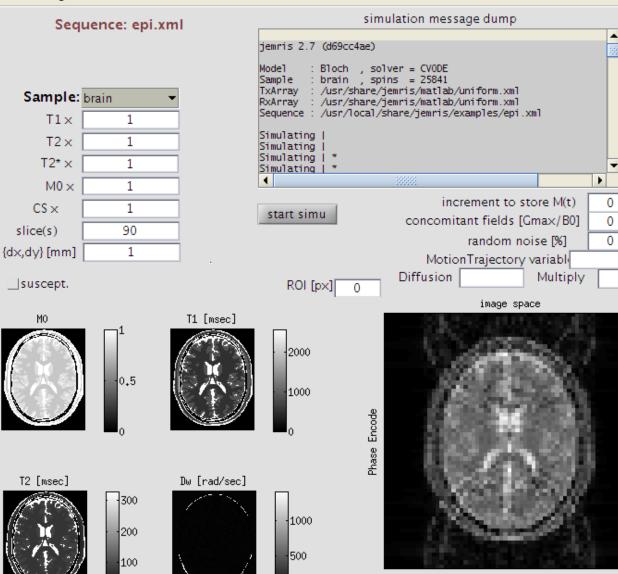
in advanced softwares



What we expect (angiographic images)

#### 😕 🗐 🔲 JEMRIS: Simulation

#### File Settings



Readout (Freq. Enc.)

JEMRIS Version 2.7 Copyright (C) 2006-2013 Tony Stöcker, Kaveh Vahedipour, Daniel Pflugfelder

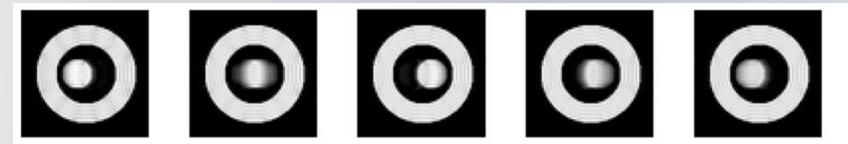
Forschungszentrum Jülich, Deutschland

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#### **Limit of motions in Jemris**

Only rigid motion of the whole sample (eg to simulate a

movement of the patient).



**Oscillating sphere** (from Stöcker T, Vahedipour K, Pflugfelder D, Shah NJ. High-performance computing MRI simulations.

Magn Reson Med. 2010 Jul,64(1):186-93)

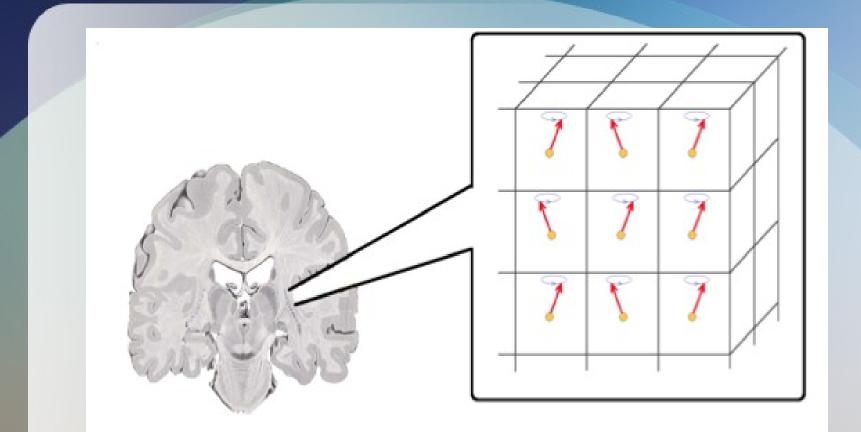
**Simulate MRI = Simulate evolution of macroscopic** 

magnetization of tissues, ie solve an ODE (Bloch equation) in

every point of the sample.

 $\frac{d\vec{M}}{dt} = \gamma \vec{M} x \vec{B}$ 

(... plus a relaxation term)



**Isochromat Summation** 

#### And for flow motion ?

$$\frac{\partial \vec{M}}{\partial t} + (\vec{V}, \vec{\nabla}) \vec{M} = \gamma \vec{M} x \vec{B}$$

(... plus relaxation term)

We could express Bloch equation considering velocity in

each point. But resolution becomes more complex (PDE).

**Eulerian approach** 

#### And for flow motion ?

$$\frac{d\vec{M}}{dt} = \gamma \vec{M} x \vec{B}$$

(... plus relaxation term)

Otherwise, keep the same equation but make evolve the

position of each flow particle over time.

#### And for flow motion ?

$$\frac{d\vec{M}}{dt} = \gamma \vec{M} x \vec{B}$$

(... plus relaxation term)

 $r = r_i(t) \implies B(t) = B_o + G(t).r_i(t)$ 

#### And for flow motion ?

$$\frac{d\vec{M}}{dt} = \gamma \vec{M} x \vec{B}$$

(... plus relaxation term)

Advantages : Easy to solve, flexible, possibility to simulate

contrast agent injection.

### **Limit of motions in Jemris**

One unique trajectory can be specified for the whole

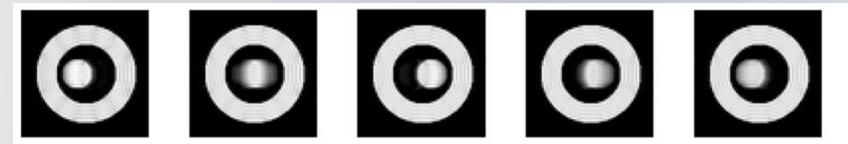
sample in Jemris...

but...

#### **Limit of motions in Jemris**

Only rigid motion of the whole sample (eg to simulate a

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### **Limit of motions in Jemris**

One unique trajectory can be specified for the whole

sample in Jemris...

but...

Simulating flow motion suppose to know the individual

trajectory of each particle.

### **Limit of motions in Jemris**

=> Necessity to *modify Jemris code* in order to take

multiple trajectories as input

Simulating flow motion suppose to know the individual

trajectory of each particle.

#### And for flow motion ?

$$\frac{d\dot{M}}{dt} = \gamma \vec{M} x \vec{B} \quad (\dots \text{ plus relaxation term})$$

 $r = r_i(t) \implies B(t) = B_o + G(t).r_i(t)$ 

### **FIRST RESULTS**

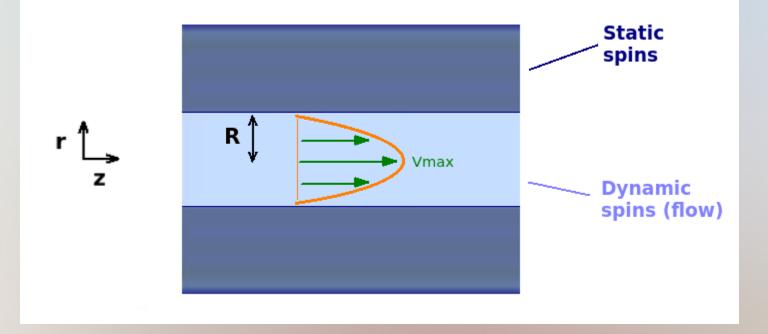
IEMBIC: Cir

#### Simple test : 4 spins with 4 different trajectories

File Settings	لا ا
Sequence:	simulation message dump
	empty 🔺
Sample: 2D sphere 👻	
T1 [ms] 1000	
T2 [ms] 100	
T2* [ms] 100	
M0 1	
CS [rad/s] 0	start simu soncemitant fields (Cmax (P0)
Radius [mm] 50	concomitant fields [Gma×/B0] 0 random noise [%] 0
{dx,dy} [mm] 1	MotionTrajectory variable
· · ·	Diffusion
	ROI [px] 0 image space
MO T1 [msec]	Tundae sharee
	1000
0.5	500
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T2 [msec] Dw [rad/sec]	1 × ×
	10.5
50	
30	-0.5
× ·	EPI reordering?
Sample 👻	_]zoom Image
Sampra	

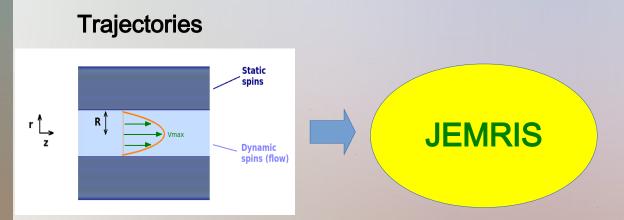


Input data : Synthetic trajectories of Poiseuille.



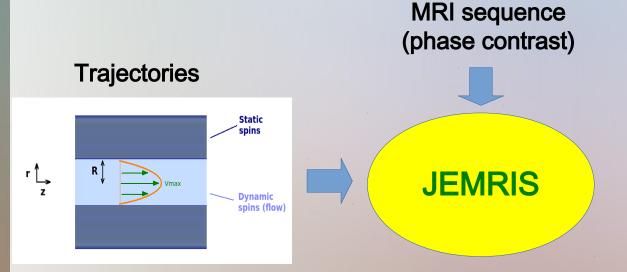


Input data : Synthetic trajectories of Poiseuille.



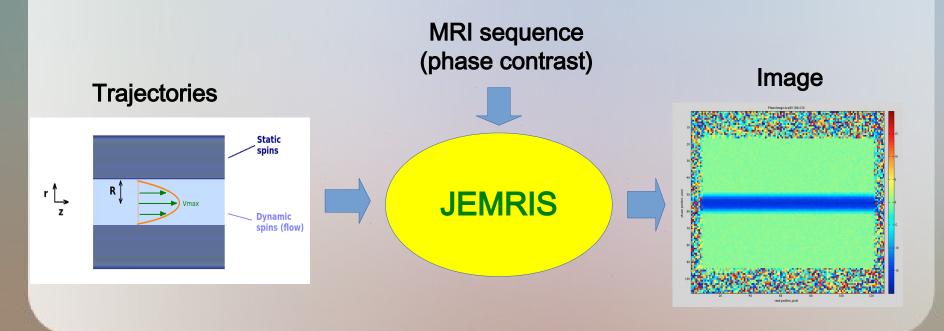


Input data : Synthetic trajectories of Poiseuille.

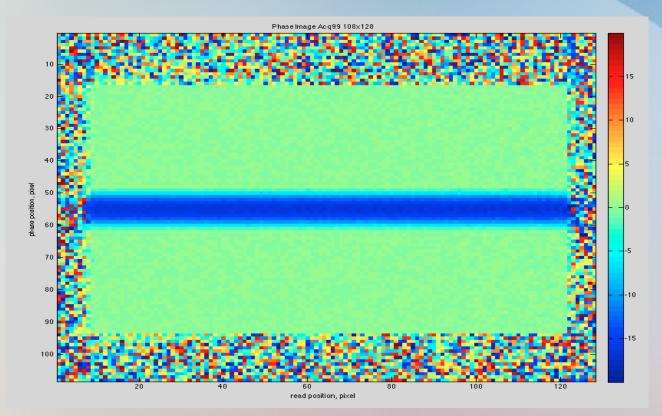




**Input data :** Synthetic trajectories of Poiseuille.





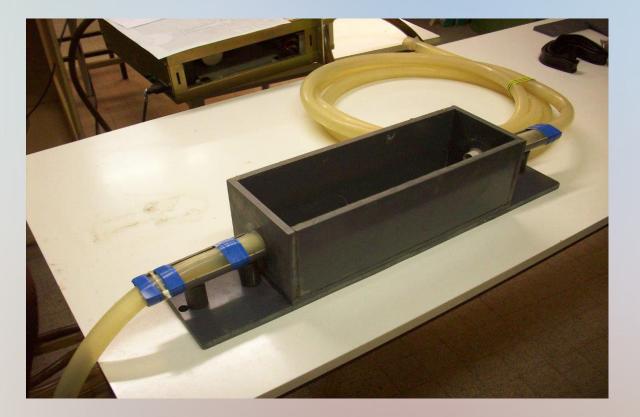


Velocity map

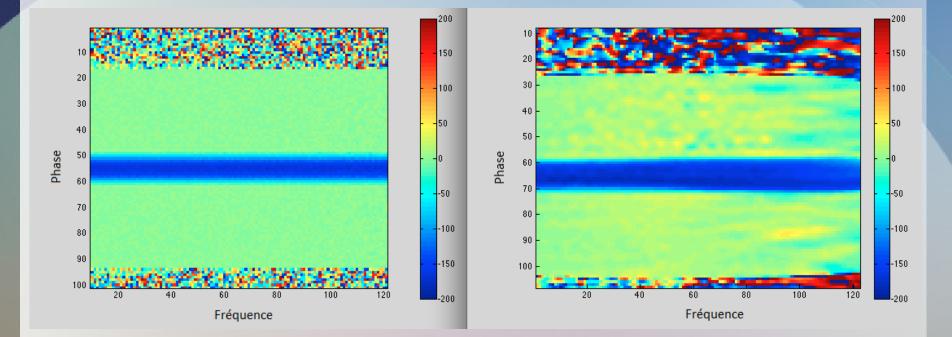


#### **Comparison to experimental images**

Hydrodynamic pulsed bench.



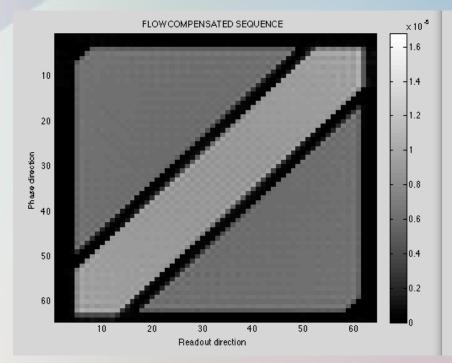
## © COMPARISON

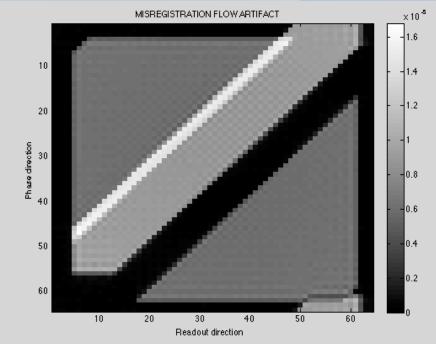


#### SIMULATION

#### HYDRO BENCH

### ♥ OTHER SIMULATIONS : FLOW ARTIFACTS

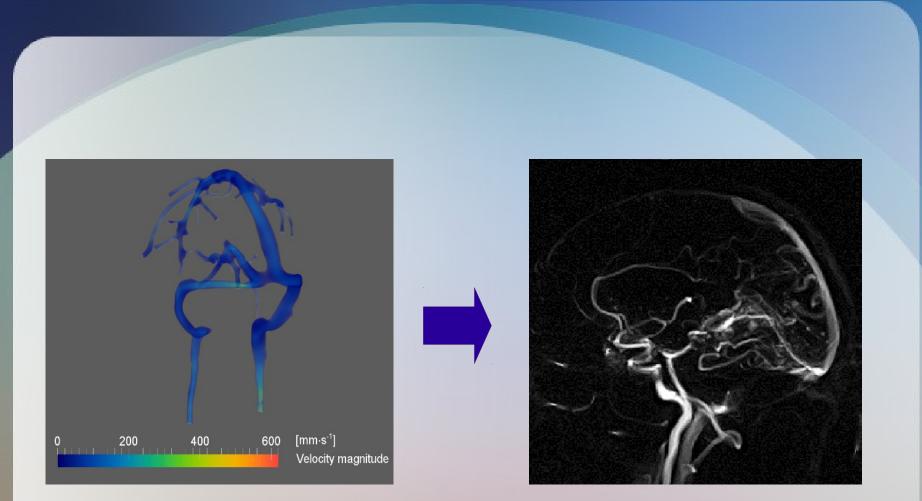




« Normal » image with flow compensation

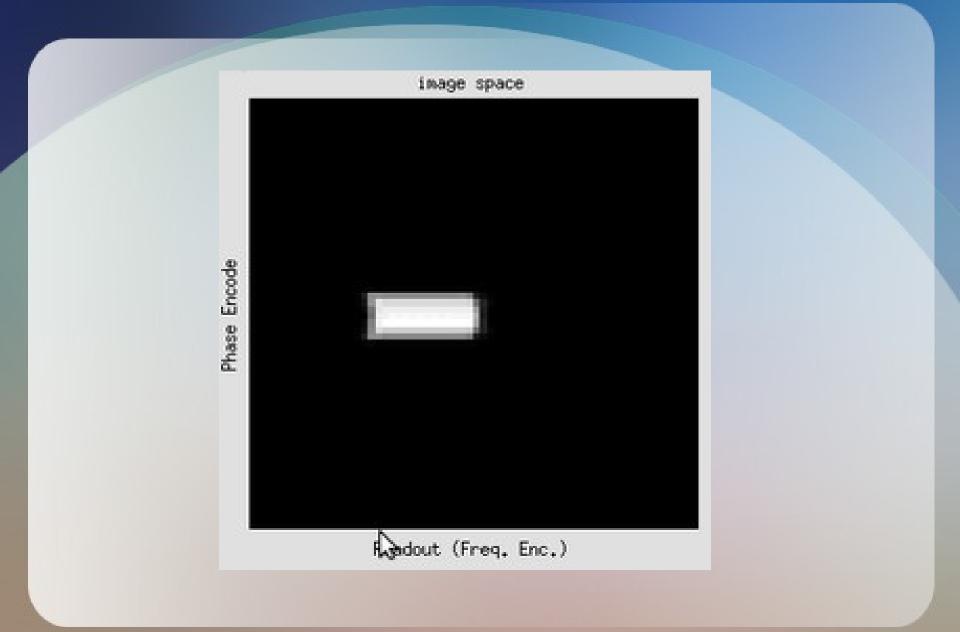
Misregistration artifact with uncompensated sequence





Simulate images of *cerebral vasculature* with velocities obtained by *Computational Fluid Dynamic* (numerical solving of Navier-Stokes equations)







→ Use Jemris to study errors in PC concerning flow rate and vessels diameter measurement

→ Eventually couple this measures with other well-known source of errors, such as concomitant fields or non uniform gradients



#### THANK YOU !

AND THANKS TO JEMRIS DEVELOPERS...

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Jemris website: http://www.jemris.org